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by

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VALIDATION OF AN OPEN SOURCE FRAMEWORK FOR THE SIMULATION OF BLOOD FLOW IN RIGID AND DEFORMABLE VESSELS

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ABSTRACT. We discuss in this paper the validation of an open source framework for the solution of problems arising in hemodynamics. The proposed framework is assessed through experimental data for steady flow in an idealized medical device with rigid boundaries and a numerical benchmark for flow in compliant vessels. The core of the framework is an open source parallel finite element library that features several algorithms to solve both fluid and fluid-structure interaction problems. The numerical results for the flow in the idealized medical device (consisting of a conical convergent, a narrow throat, and a sudden expansion) are in good quantitative agreement with the measured axial components of the velocity and pressures for three different flow rates corresponding to laminar, transitional, and turbulent regimes. We emphasize the crucial role played by the accuracy in performing numerical integration, mesh, and time step to match the measurements. The numerical fluid-structure interaction benchmark deals with the propagation of a pressure wave in a fluid-filled elastic tube. The computed pressure wave speed and frequency of oscillations, and the axial velocity of the fluid on the tube axis are close to the values predicted by the analytical solution associated with the benchmark. A detailed account of the methods used for both benchmarks is provided.

1. INTRODUCTION

Computational fluid dynamics (CFD) is nowadays a tool of choice for the investigation of blood flow problems. It has been extensively applied over the years to the study the physiology and pathophysiology of the cardiovascular system [1, 2, 3] and to patient-specific planning of interventions for cardiovascular disease [4, 5, 6]. It has been used in the medical device industry to develop and/or analyze the performance of prosthetic heart valves [7], stents [8, 9], ventricular assist devices [10], blood filters [11] etc. In addition, CFD results are also being used by some manufacturers to help demonstrate safety and efficacy of a device as part of the pre-market device submissions to the U.S. Food and Drug Administration (FDA) [12].

Key words and phrases. Computational fluid dynamics; hemodynamics; experimental validation; fluid-structure interaction.

However, the reliability of the computational approach to the study of physics phenomena is dependent on the *validation* of the mathematical models and the *verification* of the numerical methods [13]. A verified method is capable of correctly solving the problem equations, while a valid model is able to correctly describe the features of the problem (i.e. it uses the right equations).

In 2004, the FDA launched a “Critical Path Initiative” program [14] aimed, among other things, at improving the use and validating CFD techniques in the evaluation of medical devices. A benchmark nozzle model was developed which contains all the features commonly encountered in medical devices (flow contraction and expansion, recirculation zones etc., see Figure 1) and three laboratories were asked to perform flow visualization experiments on fabricated models for five flow rates spanning laminar, transitional, and turbulent regimes [12]. This resulted in benchmark data available online to the scientific community for the validation of CFD simulations [15]. Other significant efforts towards the definition of a shared test bed for numerical solvers for partial differential equations, and specifically for flow problems, include the works by Turek and coworkers for the verification of solvers for the Navier-Stokes equations [16] and for the fluid-structure interaction problem [17, 18].

The results of a first CFD study of the FDA nozzle model are reported in [19]. Twenty-eight groups of CFD professionals around the world participated in the study, following different modeling approaches (turbulence models vs. direct numerical simulations, 2D vs. 3D geometries, choice of the boundary conditions etc). Overall, the results obtained by different groups had a very large variability, also with respect to the experimental results. It was observed that turbulence models were in general unable to correctly estimate the centerline velocities in the inlet and throat of the nozzle, and velocities and shear stresses in the recirculation zones downstream of the sudden expansion. Limitations of direct numerical simulations when dealing with flows in the transitional regime were also discussed, most likely due to under-resolution of the computational grid. One of the conclusions of the study was the recommendation that validation studies should always be performed when attempting the use of computational models for the evaluation of medical devices.

Our goal is two-fold: (i) validate an open source CFD framework for the solution of problems of interest in hemodynamics and (ii) provide a detailed report on the methodology that we use, to make our experiences reproducible. To achieve this goal we refer to (a) the FDA benchmark; (b) a FSI test case presented in [20]. The former is intended to assess the code capabilities in simulating steady fluid flow in a rigid domain representative of a medical device. The latter is intended to evaluate the performance of the software in simulating fluid flow in deformable domains, which is clearly of utmost relevance for cardiovascular problems. In particular - in absence of a FSI analogue of the FDA benchmark - the FSI test deals with the propagation of a pressure wave in a fluid-filled elastic cylindrical vessel for which an analytical solution for the wave speed and frequency of oscillation are provided.

The core of our open-source CFD framework is LifeV [21], an open source library of algorithms and data structures for the numerical solution of partial differential equations with high performance computing (HPC) technologies; LifeV is a C++ software project distributed under the LGPL license. High performance computing is supported by LifeV through the interplay with third-party software (in particular

the linear algebra package Trilinos [22] by Sandia National Laboratories). LifeV is maintained and developed by an international network of universities and research centers across Europe and the US, whose core members are the Politecnico di Milano (Italy), the École Polytechnique Fédérale de Lausanne (Switzerland), and Emory University in Atlanta (USA). Other institutions contribute to the project, including the INRIA in Paris (France), Florida State University, Georgia Institute of Technology, and the University of Houston.

LifeV has been used over the last ten years as a valuable tool for the prototyping of numerical methods (see e. g. [23, 24, 25, 26, 27, 28]). Moreover, software based on LifeV has been extensively used in research projects focused on the modeling of blood flow problems, among others the drug release from implantable stents [29], the design of medical procedures in cardiology [30], the optimization of diagnostic procedures [31], surgical planning [32] and the study of cerebral hemodynamics [33].

As part of the framework we also consider open source mesh generators, such as Netgen [34] and Gmsh [35], and software for visualization and post processing such as ParaView [36]. Both Netgen and Gmsh provide several algorithms for 3D mesh generation and mesh refinement. Their scripting languages allow to have a fine control on the features of the mesh when dealing with simple geometries (in particular axisymmetric domains). Netgen is distributed under the LGPL license and Gmsh under the GPL license. ParaView is a large software project based on VTK. In this context, it is recalled for its powerful graphical interface and for offering several filters to operate on the data from numerical simulation (to visualize, probe, process, ...). ParaView is released under its own (BSD-style) ParaView License.

We discuss in this paper some of the the strengths of this framework, such as its open source nature, its solid mathematical background, its flexibility in handling complex geometries, and its performance on HPC machines. This work in fact represents a first step towards making such CFD framework a reliable tool for flow simulations in medical devices or biomechanics problems. Nonetheless, we also draw some conclusions (e.g. on which methods and algorithms work best in the different flow regimes) that are not restricted to this specific CFD framework, but rather are general and could be used as guidelines for similar CFD studies with different software.

The outline of the paper is as follows. In Section 2 we state the problems that we want to solve (fluid, structure, and coupled fluid-structure interaction problems). For each problem we touch on the numerical methods that we use for their discretization in time and space and discuss the solution of the associated linear systems. In Section 3, we describe the FDA benchmark and the numerical benchmark for FSI problems and we report the results of the validation and verification. Conclusions are drawn in Section 4.

2. PROBLEM DEFINITION

2.1. The fluid equations. The motion of an incompressible viscous fluid in a spatial domain (denoted hereafter by Ω_f) over a time interval of interest (t_0, T) is

described by the Navier-Stokes equations

$$(1) \quad \rho_f \left(\frac{\partial \mathbf{u}}{\partial t} + (\mathbf{u} \cdot \nabla) \mathbf{u} \right) - \nabla \cdot \boldsymbol{\sigma}_f = \mathbf{g}_f \quad \text{in } \Omega_f \times (t_0, T),$$

$$(2) \quad \nabla \cdot \mathbf{u} = 0 \quad \text{in } \Omega_f \times (t_0, T),$$

where ρ_f is the fluid density, \mathbf{u} is the fluid velocity, $\boldsymbol{\sigma}_f$ the Cauchy stress tensor and \mathbf{g}_f the body force. For Newtonian fluids $\boldsymbol{\sigma}_f$ has the following expression

$$\boldsymbol{\sigma}_f(\mathbf{u}, p) = -p\mathbf{I} + 2\mu_f \boldsymbol{\epsilon}(\mathbf{u}),$$

where p is the pressure, μ_f is the fluid dynamic viscosity, and $\boldsymbol{\epsilon}(\mathbf{u}) = (\nabla \mathbf{u} + (\nabla \mathbf{u})^T)/2$ is the strain rate tensor. Equations (1)-(2) need to be supplemented with initial and boundary conditions.

In the following we focus on the problem of the flow of blood in a vessel (either rigid or deformable). For such a problem, it is commonly accepted to ignore any body force (including the gravity force).

The Reynolds number can be used to characterize the flow regime, and identify the transition of the flow to turbulence. We define the Reynolds number as

$$(3) \quad Re = \frac{\bar{u}D}{\nu_f}$$

where \bar{u} is the mean sectional velocity within a pipe of hydraulic diameter D and $\nu_f = \mu_f/\rho_f$ is the fluid kinematic viscosity. The Reynolds number can be thought of as the ratio of inertial forces to viscous forces. For large Reynolds numbers, inertial forces are dominant over viscous forces and *vice versa*.

2.1.1. Discretization. We approximate in time equations (1)-(2) by the backward differentiation formula of order 2 (BDF2 [37]) and we linearize the convective term by an extrapolation formula of the same order. Given $\Delta t \in \mathbb{R}$, let us set $t^n = t_0 + n\Delta t$, with $n = 0, \dots, N_T$ and $T = t_0 + N_T\Delta t$. Problem (1)-(2) discretized in time reads: given \mathbf{u}^n , for $n \geq 1$, find the solution $(\mathbf{u}^{n+1}, p^{n+1})$ of the system:

$$(4) \quad \rho_f \frac{3\mathbf{u}^{n+1} - 4\mathbf{u}^n + \mathbf{u}^{n-1}}{2\Delta t} + \rho_f (2\mathbf{u}^n - \mathbf{u}^{n-1}) \cdot \nabla \mathbf{u}^{n+1} - \nabla \cdot \boldsymbol{\sigma}_f(\mathbf{u}^{n+1}, p^{n+1}) = \mathbf{0} \quad \text{in } \Omega_f,$$

$$(5) \quad \nabla \cdot \mathbf{u}^{n+1} = 0 \quad \text{in } \Omega_f.$$

For the space discretization, we introduce a conformal and quasi-uniform partition \mathcal{T}_h^f of Ω_f made up of a certain number of tetrahedra. We will use two inf-sup stable finite element pairs: the \mathbb{P}_1^b - \mathbb{P}_1 elements and the \mathbb{P}_2 - \mathbb{P}_1 elements and we will point out the strengths and limitations of both. For more details concerning the discretization of the Navier-Stokes problem, we refer, e.g., to [38].

Let us denote by M the mass matrix, K the stiffness matrix, N the matrix associated with the discretization of the convective term, and B the matrix associated with the discretization of the operator $(-\nabla \cdot)$. The linearization and full discretization of problem (1)-(2) yields the following system

$$(6) \quad \rho_f \frac{3}{2\Delta t} M \mathbf{u}^{n+1} + \mu_f K \mathbf{u}^{n+1} + \rho_f N \mathbf{u}^{n+1} + B^T \mathbf{p}^{n+1} = \mathbf{b}_u^{n+1},$$

$$(7) \quad B \mathbf{u}^{n+1} = \mathbf{0},$$

where \mathbf{u}^{n+1} and \mathbf{p}^{n+1} are the arrays of nodal values for velocity and pressure. The array \mathbf{b}_u^{n+1} accounts for the contributions of solution at the previous time steps and the contribution that the boundary nodes give to the internal nodes.

Set $C = \rho_f \frac{3}{2\Delta t} M + \mu_f K + \rho_f N$. We can rewrite (6)-(7) in the form

$$(8) \quad A\mathbf{x}^{n+1} = \mathbf{b}_f^{n+1},$$

where

$$(9) \quad A = \begin{bmatrix} C & B^T \\ B & 0 \end{bmatrix}, \quad \mathbf{x}^{n+1} = \begin{bmatrix} \mathbf{u}^{n+1} \\ \mathbf{p}^{n+1} \end{bmatrix}, \quad \mathbf{b}_f^{n+1} = \begin{bmatrix} \mathbf{b}_u^{n+1} \\ \mathbf{0} \end{bmatrix}.$$

At every time level t^{n+1} , to solve system (8) we use the left preconditioned GMRES method. As preconditioner, we use an upper-triangular variant of the pressure corrected Yosida splitting [23, 39] given by

$$(10) \quad P = \begin{bmatrix} C & B^T \\ 0 & S(S + BH(\mu_f K + \rho_f N)HB^T)^{-1}S \end{bmatrix}, \quad H = \frac{2\Delta t}{3\rho_f} M^{-1}, \quad S = -BHB^T.$$

The above preconditioner is a suitable approximation of the U factor in the exact block LU factorization of matrix A in (9):

$$(11) \quad A = LU, \quad L = \begin{bmatrix} I & 0 \\ BC^{-1} & I \end{bmatrix}, \quad U = \begin{bmatrix} C & B^T \\ 0 & -BC^{-1}B^T \end{bmatrix}.$$

See also [40, 41, 42] for more details.

2.2. The structure equations. The motion of an elastic structure in terms of its displacement field \mathbf{d} with respect to a given material reference configuration $\widehat{\Omega}_s$ is governed by the elastodynamics equation

$$(12) \quad \rho_s \frac{\partial^2 \mathbf{d}}{\partial t^2} - \nabla \cdot \boldsymbol{\Sigma}_s(\mathbf{d}) = \mathbf{g}_s \quad \text{in } \widehat{\Omega}_s \times (t_0, T),$$

where \mathbf{g}_s is the body force which we neglect in the following. We assume that the structure behaves like a linearly elastic, or Hookean, material. Thus, we have:

$$(13) \quad \boldsymbol{\Sigma}_s(\mathbf{d}) = 2\mu_s \boldsymbol{\epsilon}(\mathbf{d}) + \lambda_s (\nabla \cdot \mathbf{d}) \mathbf{I},$$

Here, $\boldsymbol{\epsilon}(\mathbf{d}) = (\nabla \mathbf{d} + (\nabla \mathbf{d})^T)/2$ is the strain tensor, μ_s and λ_s are the Lamé constants, that are related to Young's modulus E and the Poisson ratio ν_s as follows:

$$\mu_s = \frac{E}{2(1 + \nu_s)}, \quad \lambda_s = \frac{E\nu_s}{(1 + \nu_s)(1 - 2\nu_s)}.$$

2.2.1. Discretization. For the time discretization of problem (12), we adopt a method from the family of generalized- α schemes (see, e.g., [43]). Such schemes represent a more stable version of the well-known Newmark method

$$(14) \quad \rho_s \mathbf{a}^{n+1} - \nabla \cdot \boldsymbol{\sigma}_s(\mathbf{d}^{n+1}) = \mathbf{0},$$

$$(15) \quad \mathbf{d}^{n+1} = \mathbf{d}^n + \Delta t \mathbf{v}^n + \Delta t^2 \left(\beta \mathbf{a}^{n+1} + \left(\frac{1}{2} - \beta \right) \mathbf{a}^n \right),$$

$$(16) \quad \mathbf{v}^{n+1} = \mathbf{v}^n + \Delta t (\gamma \mathbf{a}^{n+1} + (1 - \gamma) \mathbf{a}^n),$$

where \mathbf{v}^n and \mathbf{a}^n are proper approximations of the structure velocity and acceleration at time t^n . Here, set $\beta = \frac{1}{4}$ and $\gamma = \frac{1}{2}$ to have second order accuracy. The numerical solutions obtained with the Newmark scheme may be affected by high frequency spurious oscillations if the time step is not small enough compared to the

space discretization parameters. Generalized- α methods act as low-pass filters that selectively introduce numerical damping only for the high frequency modes, while conserving the low frequency modes. The spectral properties of those methods are determined by a single parameter: the asymptotic spectral radius ρ_∞ ($0 \leq \rho_\infty \leq 1$). If $\rho_\infty = 1$ the generalized- α method reduces to the Newmark method. By setting

$$(17) \quad \mathbf{a}^{n+1-\alpha_m} = (1 - \alpha_m(\rho_\infty))\mathbf{a}^{n+1} + \alpha_m(\rho_\infty)\mathbf{a}^n, \quad 0 \leq \alpha_m(\rho_\infty) \leq 1$$

$$(18) \quad \mathbf{d}^{n+1-\alpha_k} = (1 - \alpha_k(\rho_\infty))\mathbf{d}^{n+1} + \alpha_k(\rho_\infty)\mathbf{d}^n, \quad 0 \leq \alpha_k(\rho_\infty) \leq 1,$$

the generalized- α scheme replaces momentum equation (14) by

$$(19) \quad \rho_s \mathbf{a}^{n+1-\alpha_m} - \nabla \cdot \boldsymbol{\sigma}_s(\mathbf{d}^{n+1-\alpha_k}) = \mathbf{0}.$$

By using (17)-(18) and (15)-(16), it is possible to rewrite equation (19) in terms of the only unknown \mathbf{v}^{n+1} . Concerning the particular choice of the generalized- α method and parameters, we take $\alpha_m = -1$, $\alpha_k = 0$, $\gamma = 3/2$ and $\beta = 1$, which correspond to $\rho_\infty = 0$. This scheme, originally proposed in [44], features excellent stability properties and second order of accuracy in time.

For the space discretization, we introduce a conformal and quasi-uniform triangulation \mathcal{T}_h^s of $\widehat{\Omega}_s$ made up of a certain number of tetrahedra and we set up a Galerkin finite element procedure using \mathbb{P}_2 elements. We denote by M_s the mass matrix and by K_s the stiffness matrix obtained after discretization of problem (12). The problem now becomes: given \mathbf{v}^n , for $n \geq 1$, find the solution \mathbf{v}^{n+1} of equation:

$$D\mathbf{v}^{n+1} = \mathbf{b}_s^{n+1}, \quad \text{with} \quad D = \rho_s \frac{1 - \alpha_m}{\gamma \Delta t} M_s + (1 - \alpha_k) \frac{\beta}{\gamma} \Delta t K_s,$$

where \mathbf{v} is the array of nodal values for the structure velocity, while \mathbf{b}_s accounts for the contributions of the solution at the previous time steps and boundary conditions.

2.3. The coupled problem. The structure deforms due to the contact force exerted by the fluid onto the fluid-structure interface, so that both the structure and fluid domains depend on t , i. e. $\Omega_s = \Omega_s(t)$ and $\Omega_f = \Omega_f(t)$. Let us denote by $\Gamma(t)$ the fluid-structure interface, that is the common boundary between $\Omega_f(t)$ and $\Omega_s(t)$. At $\Gamma(t)$, the fluid problem (1)-(2) and the structure problem (12) are coupled by two transmission conditions:

(1) continuity of velocity

$$(20) \quad \mathbf{u} = \mathbf{v} \quad \text{on } \Gamma(t) \times (t_0, T);$$

(2) continuity of stress

$$(21) \quad \boldsymbol{\sigma}_f \mathbf{n} = \boldsymbol{\sigma}_s \mathbf{n} \quad \text{on } \Gamma(t) \times (t_0, T),$$

\mathbf{n} being the outward normal for $\Omega_f(t)$. In (21), $\boldsymbol{\sigma}_s$ is the structure Cauchy stress tensor, which is the Eulerian description of the second Piola-Kirchhoff stress tensor $\boldsymbol{\Sigma}_s$ defined in (13).

In order to describe the evolution of the whole domain $\Omega(t) = \Omega_f(t) \cup \Omega_s(t)$, we adopt two different approaches in each subdomain. The structure domain is described with a Lagrangian mapping as in section 2.2. Thus, if $\mathbf{d} : \widehat{\Omega}_s \times (t_0, T)$ denotes the displacement of the structure with respect to the reference configuration, then each point \mathbf{x}_s in the current configuration $\Omega_s(t)$ is associated to a point $\widehat{\mathbf{x}}_s$ in the reference configuration by $\mathbf{x}_s(\widehat{\mathbf{x}}_s, t) = \widehat{\mathbf{x}}_s + \mathbf{d}(\widehat{\mathbf{x}}_s, t)$. The fluid domain is described with an *Arbitrary Lagrangian-Eulerian* (ALE) mapping. In other words,

its kinematics is only required to comply by that of the boundary $\Gamma(t)$, which is the result of the coupling with the structural model. We define the position \mathbf{x}_f of internal points to $\Omega_f(t)$ as the harmonic extension of the position of points on $\Gamma(t)$. See, e.g., [45, 46] for details. The position in the reference fluid domain $\widehat{\Omega}_f$ (at $t = 0$) is denoted by $\widehat{\mathbf{x}}_f$, and the domain velocity \mathbf{w} is calculated using the following expression:

$$\mathbf{w}(\mathbf{x}_f, t) = \left. \frac{\partial \mathbf{x}_f}{\partial t} \right|_{\widehat{\mathbf{x}}_f}.$$

The velocity ALE time derivative, i. e. rate of change of the fluid velocity in a point that moves with the computational domain reads

$$\left. \frac{\partial \mathbf{u}}{\partial t} \right|_{\widehat{\mathbf{x}}_f} = \frac{\partial \mathbf{u}}{\partial t} + \mathbf{w} \cdot \nabla \mathbf{u}.$$

With these definitions, we can write the incompressible Navier-Stokes equations in ALE formulation as follows:

$$(22) \quad \rho_f \left. \frac{\partial \mathbf{u}}{\partial t} \right|_{\widehat{\mathbf{x}}_f} + \rho_f (\mathbf{u} - \mathbf{w}) \cdot \nabla \mathbf{u} - \nabla \cdot \boldsymbol{\sigma}_f = \mathbf{0} \quad \text{in } \Omega_f(t) \times (t_0, T),$$

$$(23) \quad \nabla \cdot \mathbf{u} = 0 \quad \text{in } \Omega_f(t) \times (t_0, T).$$

Coupling conditions (20),(21) can be written in the equivalent form

$$(24) \quad r_f \mathbf{u} + \boldsymbol{\sigma}_f \mathbf{n} = r_f \mathbf{v} + \boldsymbol{\sigma}_s \mathbf{n} \quad \text{on } \Gamma(t) \times (t_0, T),$$

$$(25) \quad r_s \mathbf{u} + \boldsymbol{\sigma}_f \mathbf{n} = r_s \mathbf{v} + \boldsymbol{\sigma}_s \mathbf{n} \quad \text{on } \Gamma(t) \times (t_0, T),$$

where $r_f > 0$ and $r_s > 0$ ($r_f \neq r_s$) are constants.

2.3.1. *Discretization.* At every time level t^{n+1} , the FSI problem discretized in time and space can be written in matrix form as:

$$(26) \quad A_{fs} \mathbf{x}_{fs}^{n+1} = \mathbf{b}_{fs}^{n+1},$$

$$(27)$$

$$A_{fs} = \begin{bmatrix} C + r_f R_f & T_{fs} & B^T \\ T_{su} & D + r_s R_s & T_{sp} \\ B & 0 & 0 \end{bmatrix}, \quad \mathbf{x}_{fs}^{n+1} = \begin{bmatrix} \mathbf{u}^{n+1} \\ \mathbf{v}^{n+1} \\ \mathbf{p}^{n+1} \end{bmatrix}, \quad \mathbf{b}_{fs}^{n+1} = \begin{bmatrix} \mathbf{b}_u^{n+1} \\ \mathbf{b}_s^{n+1} \\ \mathbf{0} \end{bmatrix}.$$

Here, the boundary mass matrices R_f , R_s and the coupling matrices T_{fs} , T_{su} , T_{sp} arise from the discretization of the coupling conditions (24),(25).

To precondition system (26), we consider an inexact LU block factorization of the matrix A_{fs} , in a similar way to what already done in Sec. 2.1 and in the same spirit of [45, 46]. The approximated U factor for matrix A_{fs} is:

$$\widehat{U}_{fs} = \begin{bmatrix} C + r_f R_f & T_{fs} & B^T \\ 0 & \widehat{\Sigma}_s & T_{sp} \\ 0 & 0 & \widehat{\Sigma}_p \end{bmatrix},$$

where $\widehat{\Sigma}_s$ and $\widehat{\Sigma}_p$ are appropriate approximations of the structure Schur complement

$$\Sigma_s = D + r_s R_s - T_{su} (C + r_f R_f)^{-1} T_{fs},$$

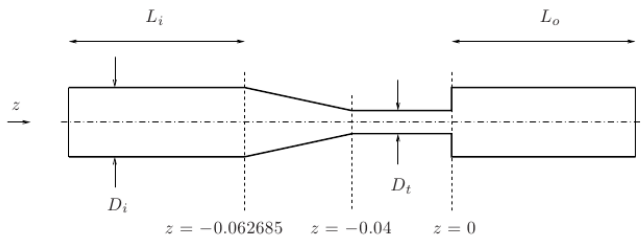


FIGURE 1. Computational domain. The units are meter.

and the pressure Schur complement

$$\begin{aligned} \Sigma_p &= -B(C + r_f R_f)^{-1} B^T + \\ & B(C + r_f R_f)^{-1} T_{fs} \Sigma_s^{-1} T_{su} (C + r_f R_f)^{-1} B^T - B(C + r_f R_f)^{-1} T_{fs} \Sigma_s^{-1} T_{sp}. \end{aligned}$$

To approximate Σ_s , we use $(C + r_f R_f)^{-1} \approx H$, where H is defined in (10). Thus, we have:

$$\widehat{\Sigma}_s = D + r_s R_s - T_{su} H T_{fs}$$

To approximate Σ_p , we use the pressure corrected Yosida preconditioner defined in Sect. 2.1:

$$(28) \quad \widehat{\Sigma}_p = S(S + BH(\mu_f K + \rho_f N)HB^T)^{-1} S.$$

At every time level t^{n+1} , we solve $\widehat{U}_{fs}^{-1} A_{fs} \mathbf{x}_{fs}^{n+1} = \widehat{U}_{fs}^{-1} \mathbf{b}_{fs}^{n+1}$ with the GMRES method. The position of the fluid domain is extrapolated from the previous time step, while the non-linearity induced by the fluid convective term is resolved with Picard iterations (see e. g. [37]).

3. RESULTS

3.1. The FDA benchmark. The FDA benchmark consists in simulating the flow of an incompressible and Newtonian fluid with prescribed density and viscosity ($\rho_f = 1056 \text{ kg/m}^3$ and $\mu_f = 0.0035 \text{ Pa}\cdot\text{s}$) in an idealized medical device shaped like a nozzle (see Fig. 1) at different Reynolds numbers.

The geometry of the device includes a conical convergent, a throat, and a sudden expansion. In this paper, we are only considering the so-called ‘‘Sudden Expansion’’ model [12, 19], that is in Fig. 1 the fluid flows from left to right. The idealized device was designed to feature accelerating, decelerating, and recirculating flow, all of which occur in real medical devices.

The system is studied in a variety of conditions, including the laminar, transient, and turbulent regimes: the results of the published inter-laboratory experiments refer to values of the Reynolds numbers (defined as in (3)) evaluated in the throat, denoted by Re_t , of $Re_t = 500, 2000, 3500, 5000, 6500$. In this paper, we focus on the first three values of Re_t for reasons that will be clarified in the following (see Remark 3.4). In table 1, we report the throat Reynolds number Re_t , the corresponding inlet Reynolds number Re_i , and flow rate for the flow regimes that we are going to consider. Notice that in all the three flow regimes the flow upstream of the throat is laminar, Re_i being below the critical Reynolds number for transitional flow in a straight pipe ($Re \simeq 2000$ [47]).

TABLE 1. Throat Reynolds number Re_t , inlet Reynolds number Re_i , and flow rate for the flow regimes under consideration.

Re_t	Re_i	flow rate Q (m ³ /s)
500	167	5.2062e-6
2000	667	2.0825e-5
3500	1167	3.6444e-5

Since we are dealing with a viscous fluid, on the lateral surface of the computational domain we prescribe a no-slip boundary condition. For all three flow regimes in table 1, at the inlet section we prescribe a Poiseuille velocity profile to get the desired flow rate, a choice which is justified by the considered values of Re_i . At the outlet section, we prescribe a stress-free (natural) boundary condition. This simulates a discharge into open air, which does not correspond to the experimental set up of the FDA benchmark (a closed flow loop [12]). However, this choice is expected to alter the computed solution only in a confined region of the computational domain close to the outlet section [48]. The results of the flow analysis are not affected, provided the computational domain represents a long enough expansion channel. As discussed in the following, we always considered the length of the expansion channel (L_o in Fig. 1) to be greater than 10 times its diameter, and we did not observe a dependence of the solution on the actual value of L_o .

As for the initial condition, we start our simulations with fluid at rest, i.e. $p = 0$ and $\mathbf{u} = \mathbf{0}$ everywhere in Ω_f . We use a smooth increase of the velocity profile at the inlet to transition from the fluid at rest to the regime flow conditions. A short transition reduces the duration and therefore the overall computational cost of the simulation. However, a fine time discretization is required to resolve fast transient dynamics of the computed solution.

For every flow regime, we use direct numerical simulations (DNS), with no turbulence model. This choice is motivated by the results presented in [19], where it is shown that DNS most accurately predicts the velocities at all Re_t , in particular in the entrance region, in the throat, and just downstream of the sudden expansion. In DNS, it is essential to assess whether or not the flow field is properly resolved. For this purpose, we follow the approach proposed by [49], that is the grid resolution is qualified in terms of the viscous length scale, computed as

$$(29) \quad l^+ = \frac{u_* \Delta l}{\nu_f}, \quad \text{with } \Delta l = 12/\sqrt{2}V_\tau^{1/3}, \quad \text{and } u_*^2 = \nu_f \|\epsilon(\mathbf{u})\|_F.$$

In (29), Δl represents the local grid size, V_τ is the tetrahedron volume, and $\|\cdot\|_F$ is the Frobenius norm. If $l^+ \sim O(1)$, the average grid size Δl is of the order of the viscous length scale, which is the smallest spatial scale at which turbulent fluctuation can persist.

Even though the semi-implicit treatment of the convective term in eq. 4 does not guarantee the unconditional stability in time of the numerical scheme, we point out that no stability issues were observed in our tests. Selection of the time step was based on accuracy considerations solely.

We compare the experimental data provided by the FDA with our numerical simulations for all the flow regimes listed in table 1. The experimental data were acquired by three independent laboratories and one of the laboratory ran three

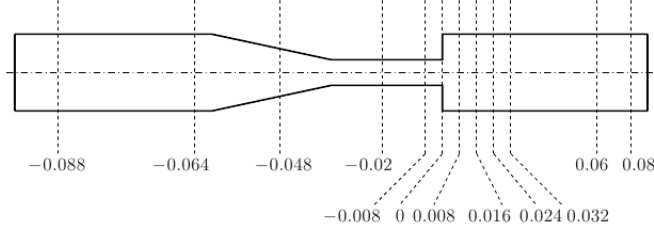


FIGURE 2. Radial sections at which the numerical results are compared against the experimental measurements.

trials, so that for each case we have five sets of data. The comparison is made in terms of normalized axial component of the velocity along the centerline and at various radial sections (see Fig. 2), and normalized wall pressure difference along the length of the domain. The axial component of the velocity u_z is normalized with respect to the average axial velocity at the inlet \bar{u}_i :

$$(30) \quad u_z^{norm} = \frac{u_z}{\bar{u}_i}, \quad \text{with} \quad \bar{u}_i = \frac{Q}{\pi D_i^2/4},$$

where Q is the volumetric flow rate calculated from the throat Reynolds number (see table 1). The pressure difference data are normalized with respect to the average velocity at the throat \bar{u}_t :

$$(31) \quad \Delta p^{norm} = \frac{p_z - p_{z=0}}{1/2 \rho_f \bar{u}_t^2}, \quad \text{with} \quad \bar{u}_t = \frac{Q}{\pi D_t^2/4},$$

where p_z denotes the wall pressure along the z axis and $p_{z=0}$ is the wall pressure at $z = 0$. As a proxy for the wall pressure at a given axial coordinate, we probed the pressure value at the corresponding location on the axis of the domain, since we observed pressure values being approximately uniform on axial cross-sections.

The graphs with the above comparisons are reported in Sec. 3.1.1 for $Re_t = 500$, Sec. 3.1.2 for $Re_t = 2000$, and Sec. 3.1.3 for $Re_t = 3500$. Finally, a quantification of the agreement is provided in Section 3.1.4 following a validation metric proposed in [19].

3.1.1. *Case $Re_t = 500$.* Among the considered values of Re_t , the case $Re_t = 500$ proved to be the the easiest to be studied, as expected since the flow is laminar all along the length of the domain.

We selected $L_i = 10D_i$ and $L_o = 15D_i$ (see Fig. 1) and considered three meshes with different levels of refinement:

- mesh *coarse15D*, obtained by setting the maximum element diameter $h = 10^{-3}$, has $6.2 \cdot 10^4$ nodes and $3.1 \cdot 10^5$ tetrahedra;
- mesh *medium15D*, obtained by setting $h = 6 \cdot 10^{-4}$, has $1.4 \cdot 10^5$ nodes and $7.5 \cdot 10^5$ tetrahedra;
- mesh *fine15D*, obtained by setting $h = 5.5 \cdot 10^{-4}$, has $2.3 \cdot 10^5$ nodes and $1.2 \cdot 10^6$ tetrahedra.

No special refinement in the convergent or throat was prescribed, nonetheless all three meshes had a small value of the viscous length scale at the steady state (maximum value $l^+ \simeq 0.5$ over the entire domain). We ran a simulation on each mesh, with time step $\Delta t = 10^{-3}$ for every mesh and using \mathbb{P}_1^b - \mathbb{P}_1 finite elements. An

advantage of this choice of finite elements is that the resulting algebraic problem is significantly smaller and easier to solve with respect to the one generated by choosing \mathbb{P}_2 - \mathbb{P}_1 finite elements. The latter are however more accurate, and this may be required in some cases, as we discuss later.

We let the simulations run until reasonably close to the steady state, which meant till $T \simeq 7$ s. This required roughly 2.5 hours of computational time on 32 CPUs for mesh *coarse15D*, 9.3 hours on 32 CPUs for mesh *medium15D*, 6.2 hours on 64 CPUs for mesh *fine15D*.

First, we report the comparison for the normalized axial velocity (30) along the z axis (Fig. 3(a)) and the normalized pressure difference (31) along the z axis (Fig. 3(b)). In Fig. 3, we plotted a dot for every measure and a solid line to linearly interpolate the five sets of measurements, while we used a dashed line for the numerical results obtained with the three meshes. From Fig. 3(a), we see that the numerical axial velocities on the three meshes are almost superimposed in the entrance region, convergent, and throat, while they differ in the sudden expansion region with decreasing difference at each refinement. Fig. 3(a) shows that the simulated axial velocities on all the meshes closely follow the measurements all along the portion of the z axis under consideration ($-0.088 \leq z \leq 0.08$). As for the numerical pressure differences, the three curves corresponding to the computational results on the three meshes are almost superimposed all along the axis (see Fig. 3(b)), but they do not match the measured data. As reported in [19], these data sets seem in fact to be significantly affected by normalization errors. This would explain the apparent positive offset of about 1.5 mmHg in most of the measurements with respect to the computed values. Moreover, the experimental results vary significantly from one data set to the other, suggesting that a comparison with the measurements might not be too meaningful in this case.

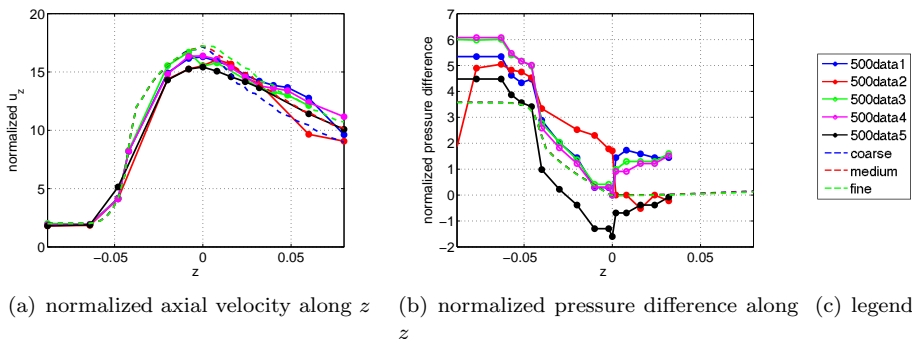


FIGURE 3. Case $Re_t = 500$: comparison between experimental data (solid lines) and numerical results (dashed lines) for (a) normalized axial velocity (30) along the z axis and (b) normalized pressure difference (31) along the z axis. The legend in (c) is common to (a) and (b).

In Fig. 4, we show the profiles of the normalized axial velocity (30) at four different radial sections. In the entrance region and in the throat (Fig. 4(a) and (b)) there is little difference between the numerical results obtained on the different meshes, indicating that no further refinement is required there. In Fig. 4(a)

and (b), a mismatch is observed between the numerical velocity profiles and the measurements. However, we point out that this is due to measurement errors. In fact, assuming axial symmetry, we can calculate the flow rate associated to each measured velocity profile. We find that the measured velocity profiles underestimate the theoretical flow rate by at least 3%, while the simulated velocity profiles retrieve the correct value within an error of 0.019% (using the fine mesh). Downstream of the sudden expansion (Fig. 4(c) and (d)), the simulated velocity profiles on the three meshes show some difference, although we can see a certain (monotonic) convergence in the shape when refining. From Fig. 4(c) and (d), we see that the simulations on meshes *medium15D* and *fine15D* match the experimental data better and are able to capture the negative velocities within the recirculation zones fairly well.

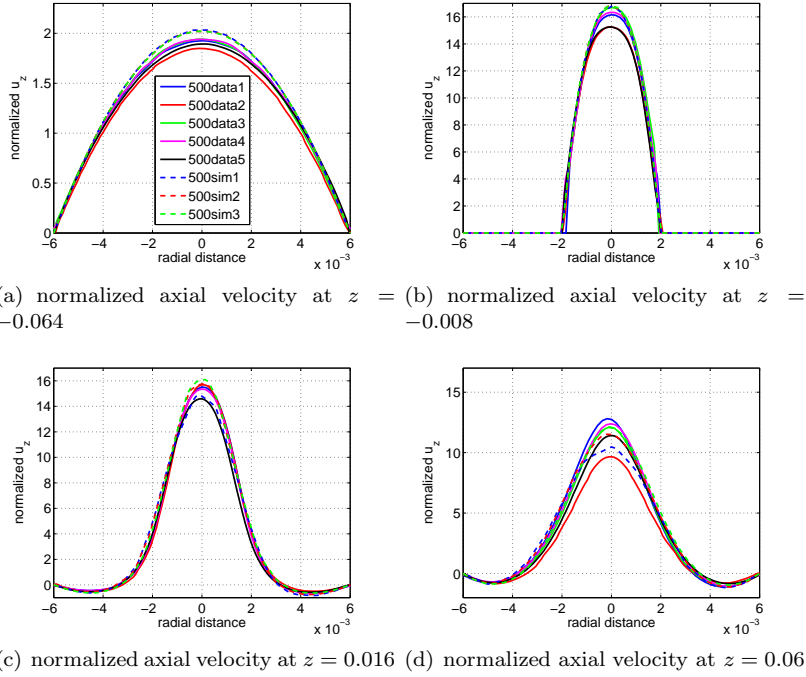


FIGURE 4. Case $Re_t = 500$: comparison between experimental data (solid lines) and numerical results (dashed lines) for normalized axial velocity (30) at (a) $z = -0.064$, (b) $z = -0.008$, (c) $z = 0.016$, and (d) $z = 0.06$. The legend in (a) is common to all four subfigures.

Remark 3.1. As mentioned in Sec. 3.1, the mesh plays a central role in DNS. At $Re_t = 500$, the flow is axially symmetric for $-0.088 \leq z \leq 0.08$. It is important that the mesh is close to uniform on each axial section to respect the symmetry of the problem. A mesh that does not have such a feature would give unphysical asymmetric velocity profile.

3.1.2. *Case $Re_t = 2000$.* The transitional regime ($Re_t = 2000$) proved to be a tough test both from the experimental and numerical point of view.

From the experimental side, the interlaboratory velocity data agreed with each other within 15% error at the entrance, convergent, throat, and right after the sudden expansion. However, farther downstream of the sudden expansion the velocity profiles from the laboratories are significantly different from one another. In particular, the experimental jet breakdown point varied among the laboratories. This was attributed mainly to a 10% higher flow rate (and consequently higher Re_t) which caused premature jet breakdown in two experiments out of five [12]. However, minor differences in the fabricated geometrical models and inlet perturbation levels played a role also. From the numerical point of view, we found the results to be very sensitive to mesh size and time step.

We selected $L_i = 10D_i$ and $L_o = 12D_i$ (see Fig. 1). After several numerical experiments, we managed to identify a mesh sufficiently refined in the different regions of the domain: maximum element diameter $h = 2 \cdot 10^{-4}$ in the throat, maximum $h = 5 \cdot 10^{-4}$ in the convergent and expansion region, maximum $h = 7 \cdot 10^{-4}$ in the entrance region, for a total of $4.6 \cdot 10^5$ nodes and $2.5 \cdot 10^6$ tetrahedra.

We set time step $\Delta t = 10^{-4}$ and used \mathbb{P}_2 - \mathbb{P}_1 finite elements. Around time $t = 0.45$ s, the turbulent regime is fully developed. The mesh viscous length scale evaluated at this time has a maximum value $l^+ \simeq 2$ over the entire domain.

We start by reporting the comparison for the normalized axial velocity (30) along the z axis (Fig. 5(a)) and the normalized pressure difference (31) along the z axis (Fig. 5(b)). In Fig. 5, we see that the simulated axial velocities and pressure differences match very well with the sets of data showing a longer jet.

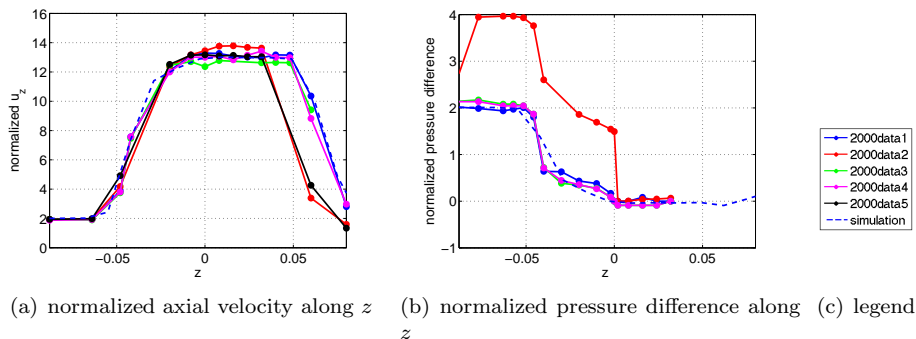


FIGURE 5. Case $Re_t = 2000$: comparison between experimental data (solid lines) and numerical results (dashed line) for (a) normalized axial velocity (30) along the z axis and (b) normalized pressure difference (31) along the z axis. The legend in (c) is common to (a) and (b).

Fig. 6 shows the profiles of the normalized axial velocity (30) at four different radial sections. As for the $Re_t = 500$ case, all the sets of measurements slightly underestimate the axial velocity at $z = -0.064$; see Fig. 6(a). Inside the throat (Fig. 6(b)), the velocity profile is plug-like. The peak velocity found by the simulation is slightly less than the ones found experimentally. In this case, the measured

velocity profiles overestimate the theoretical flow rate by at least 2%, while the simulated velocity profiles underestimate it by 0.41% (See Fig. 9(b)). Immediately downstream of the sudden expansion (Fig. 6(c)), the simulated profiles have peak values that fall within the measurements sets and the recirculation zones are pretty well captured. Section $z = 0.06$ (Fig. 6(d)) is close to the jet breakdown point for three sets of measurements, while it is past the breakdown point for the other two sets. The simulated velocity is closer to the former, as already seen in Fig. 5(a).

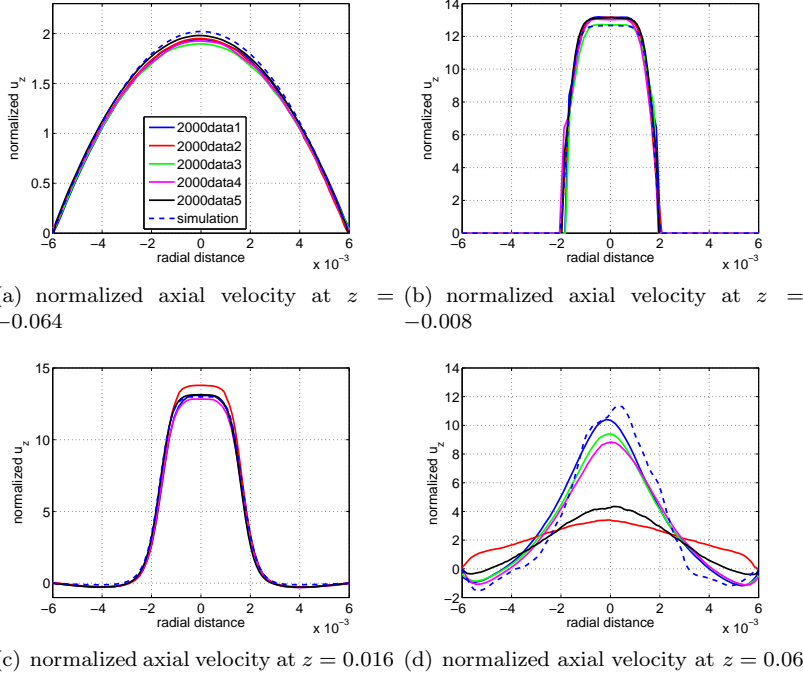


FIGURE 6. Case $Re_t = 2000$: comparison between experimental data (solid lines) and numerical results (dashed line) for normalized axial velocity (30) at (a) $z = -0.064$, (b) $z = -0.008$, (c) $z = 0.016$, and (d) $z = 0.06$. The legend in (a) is common to all four subfigures.

Remark 3.2. *The \mathbb{P}_1^b - \mathbb{P}_1 finite elements, which performed well for $Re_t = 500$, failed to give results comparable to the experimental data for $Re_t = 2000$. In the simulation at $Re_t = 2000$ with a mesh and time step similar to those used for the results in Fig. 5 and 6, the \mathbb{P}_1^b - \mathbb{P}_1 finite elements gave a numerical jet breakdown point much farther downstream than observed in the experiments. A possible cause of the mismatch with the experimental data is the accuracy of the numerical integration performed by LifeV. \mathbb{P}_1^b - \mathbb{P}_1 finite elements require the accurate evaluation of the integral of high order polynomials on the computational domain. The use of numerical methods unable to guarantee the desired accuracy may have caused the artificial damping of high frequency modes in the solution and consequently enhanced its laminar behavior.*

3.1.3. *Case $Re_t = 3500$.* The third flow regime we consider features a throat Reynolds number $Re_t = 3500$ which is well above the transitional Reynolds number in a straight channel. In fact, turbulence downstream of the sudden expansion was observed in all the experiments with a reproducible jet breakdown point, which indicates a fully turbulent flow regime.

We selected $L_i = 10D_i$ and $L_o = 15D_i$ (see Fig. 1). After numerical studies in the throat-expansion region and convergent-throat-expansion region, we managed to identify a sufficient level of refinement for the different regions of the domain: maximum element diameter $h = 1.5 \cdot 10^{-4}$ in the throat, maximum $h = 4 \cdot 10^{-4}$ in the convergent and expansion region, maximum $h = 6 \cdot 10^{-4}$ in the entrance region, for a total of $5.6 \cdot 10^5$ nodes and $3.2 \cdot 10^6$ tetrahedra.

We set time step $\Delta t = 10^{-4}$ and used \mathbb{P}_2 - \mathbb{P}_1 finite elements. Already around time $t = 0.4$ s, the turbulent regime is fully developed. The mesh viscous length scale evaluated at this time has a maximum value $l^+ \simeq 4$ over the entire domain. The simulation of 0.4 s of flow took 336 hours on 256 CPUs.

In [19], none of the presented CFD results was able to catch the jet breakdown point, because DNS predicted a longer jet (likely due to a coarse mesh) while simulations with turbulence models under-predicted the jet length. In Fig. 7(a), we see that DNS with a properly refined mesh is able to capture with precision the jet breakdown observed in the experiments. Actually, the simulated axial velocities matched with the measurements all along the portion of the z axis under consideration. As shown in Fig. 7(b), also the simulated pressure difference is in very good agreement with the experimental data, except in the convergent where the simulated pressure difference overestimates almost all the measurements.

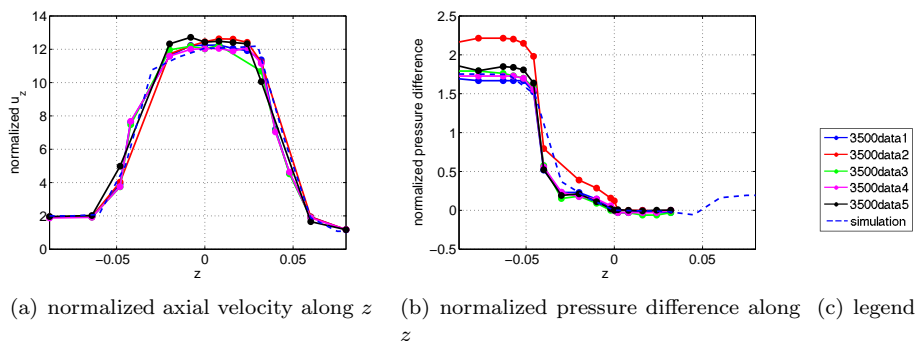


FIGURE 7. Case $Re_t = 3500$: comparison between experimental data (solid lines) and numerical results (dashed line) for (a) normalized axial velocity (30) along the z axis and (b) normalized pressure difference (31) along the z axis. The legend in (c) is common to (a) and (b).

Fig. 8 shows the profiles of the normalized axial velocity (30) at four different radial sections. The velocity profile upstream of the throat (Fig. 8(a)) is of Poiseuille type, as expected (see Re_i in table 1). The simulation results are in very good agreement in particular with one of the five data sets. Inside the throat (Fig. 8(b)), the velocity profile is plug-like. As for $Re_t = 2000$, the peak velocity found

by the simulation is a little lower than the ones found experimentally. Immediately downstream of the sudden expansion (Fig. 8(c)), the velocity profile still shows a plateau and recirculation zones appear. Here, the simulated profile has a peak that falls within the measurements sets, whereas the measurements and numerical results differ at the recirculation zones. However, it was noted in [19] that measuring velocities accurately at the wall is very hard, especially in recirculation zones downstream of the sudden expansion where velocities near the wall are low. Any conclusion about the accuracy of numerical results in that region, drawn by comparison with experimental data, has to be considered purely speculative. Section $z = 0.06$ (Fig. 8(d)) is past the jet breakdown point, thus the axial component of the velocity is much reduced. The simulated velocity captures well the magnitude of measured velocity and part of the profile.

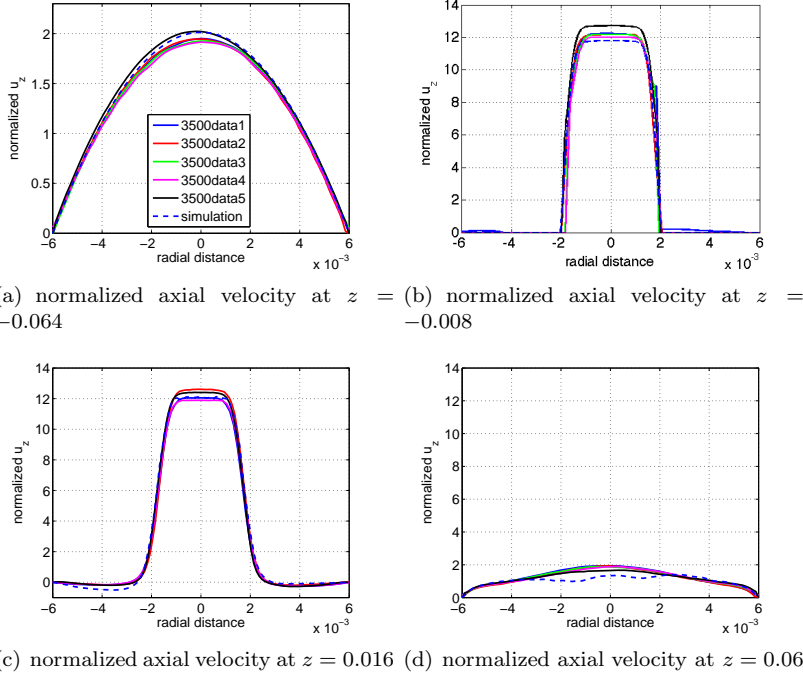


FIGURE 8. Case $Re_t = 3500$: comparison between experimental data (solid lines) and numerical results (dashed line) for normalized axial velocity (30) at (a) $z = -0.064$, (b) $z = -0.008$, (c) $z = 0.016$, and (d) $z = 0.06$. The legend in (a) is common to all four subfigures.

Remark 3.3. *Since the measurements of a turbulent flow are averaged over time [12], we averaged the numerical results. All the results presented in Fig. 7 and 8 have been averaged over 10 instants of time. We noticed that averaging over more than 10 would not change the average value.*

Remark 3.4. *Using DNS has a major limitation in the high computational costs. To fully resolve the flow features at high Reynolds number, it is necessary to consider*

TABLE 2. Validation metric E_z (32) at six radial sections upstream and inside the throat. Smaller values of the metric identify a better agreement with the available data.

	$z = -0.088$	$z = -0.064$	$z = -0.048$	$z = -0.02$	$z = -0.008$	$z = 0$
Re = 500	0.0768	0.0687	0.0516	0.0212	0.0146	0.0262
Re = 2000	0.0433	0.0384	0.0692	0.0164	0.0116	0.0127
Re = 3500	0.0343	0.0267	0.0825	0.0316	0.0212	0.0123

TABLE 3. Validation metric E_z (32) at six radial sections downstream of the throat

	$z = 0.008$	$z = 0.016$	$z = 0.024$	$z = 0.032$	$z = 0.06$	$z = 0.08$
Re = 500	0.1663	0.2639	0.2043	0.1791	0.2745	0.2591
Re = 2000	0.2662	0.4595	0.6959	1.0005	2.0609	1.1355
Re = 3500	0.7231	1.0648	0.4469	0.8729	0.4247	0.1698

simulations with a huge number of degrees of freedom [50]. Since the tests that we presented so far already show that our computational framework can simulate adequately flow in laminar, transitional and turbulent regimes, we limit our analysis of the FDA problem to Reynolds number $Re_t \leq 3500$. In the future we plan to work on turbulence models (e. g. [51, 52]) to reduce the computational costs of flow simulations in the turbulent regime.

3.1.4. *Quantitative analysis.* In order to quantify the agreement between the results of a simulation and the experimental data, in [19] a generic validation metric E_z was proposed

$$(32) \quad E_z = \frac{1}{n} \sum_{i=1}^n \left| \frac{\bar{u}_{e,i} - u_{c,i}}{\bar{u}_{e,i}} \right|,$$

where $\bar{u}_{e,i}$ is the average of the experimental velocity data at one discrete point i along the z axis, $u_{c,i}$ is the computational data at the same point i , and n is the total number of discrete points.

In tables 2 and 3, we report validation metric E_z (32) at each of the twelve radial sections in Fig. 2 taken separately for $Re_t = 500, 2000, 3500$. The corresponding graphs in semi-logarithmic scale are shown in Fig. 9(a). For $Re_t = 500$, the numerical results obtained with mesh *fine 15D* were considered (see Sec. 3.1.1).

From Fig. 9(a), we see that in the $Re_t = 500$ case the value of E_z decreases in the entrance region and in the throat, while it increases (not monotonically) in the expansion region, the maximum value being 0.2745 at $z = 0.06$ (see table 3). In the entrance region and in the throat, E_z for $Re_t = 2000$ is lower than the one for $Re_t = 500$, except at one radial section. The value of E_z increases downstream of the sudden expansion, with maximum value equal to 2.0609 at $z = 0.06$. This large value is mainly due to substantial inter laboratory variations (see Fig. 6(c)). In the $Re_t = 3500$ case, we see that the value of E_z is low in the entrance region. Then, it increases by nearly two orders of magnitude immediately downstream of the sudden expansion, with maximum value equal to 1.0648 at $z = 0.016$. It is

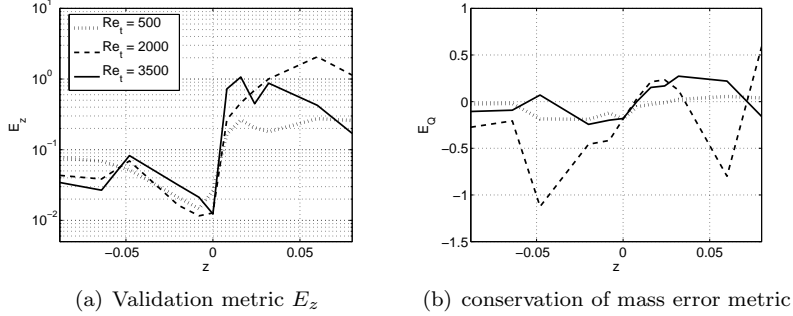


FIGURE 9. (a) Validation metric E_z (32) in semi-logarithmic scale and (b) conservation of mass error metric E_Q (33) as a function of the position along the z axis for $Re_t = 500, 2000, 3500$. The legend in (a) is common to both subfigures.

worth stressing that a large value of E_z does not necessarily reflect a significant discrepancy between computations and measures. As Fig. 8(c) shows, since the metric is a sum of normalized absolute values, the error is in general large in low-velocity regions such as recirculation zones. In fact, the computed and measured velocity values are closer than suggested by the metric.

After comparing Fig. 9(a) with the results reported in [19], we can conclude that the results presented in Sec. 3.1.1, 3.1.2, and 3.1.3 are in excellent agreement with the measurements.

For all the simulations, we evaluated also the conservation of mass at the axial positions z in Fig. 2 using the conservation of mass error metric proposed by [19], that is:

$$(33) \quad E_Q = \frac{Q_{CFD} - Q}{Q} \cdot 100,$$

where Q_{CFD} is the volumetric flow rate computed from the numerical axial velocity profiles. Higher values of this metric identify worse performances of the computational model.

Fig. 9(b) shows the conservation of mass error metric as a function of z for $Re_t = 500, 2000, 3500$. For $Re_t = 500$, the maximum error is less than 0.3%, which appears to be excellent when compared to the results reported in [19]. Thanks to the fact that the simulation on mesh *fine15D* features good mass conservation properties, we are confident that the simulated pressures in Fig. 3(b) are not far from the real pressures despite the mismatch with the experimental data. For $Re_t = 2000$, largest error (in absolute value) is inside the convergent. There, the mesh quality seems to be the key responsible, as we systematically observe some stretched elements around $z = -0.048$ in our meshes. The combination of stretched mesh elements with finite elements that are only weakly divergence-free (like the $\mathbb{P}_2 - \mathbb{P}_1$ elements we used, [53]) results in a poor approximation of the flow rate locally. Nonetheless, notice that the local validation metric E_z at $z = -0.048$ (see table 2) is satisfactory. For $Re_t = 3500$, the error (in absolute value) is below 0.5% on most of the domain, but inside the convergent. Also in this case, the problem can be attributed to the mesh quality, but we could not significantly improve on

this side without drastically increasing the number of degrees of freedom. A more careful mesh design seems to be required in regions of the domain featuring axial tapering.

3.2. The Greenshields-Weller numerical benchmark. The numerical fluid-structure interaction benchmark we are going to consider is taken from a paper by Greenshields and Weller [20]. It deals with the propagation of a pressure wave in a fluid-filled elastic tube. The geometry is selected to be representative of blood flow in large arteries: it is a straight cylindrical pipe with circular section, with length $L = 10$ cm, diameter $D = 2$ cm, and a shell of thickness $h_s = 0.2$ cm (see Fig. 10(a)).

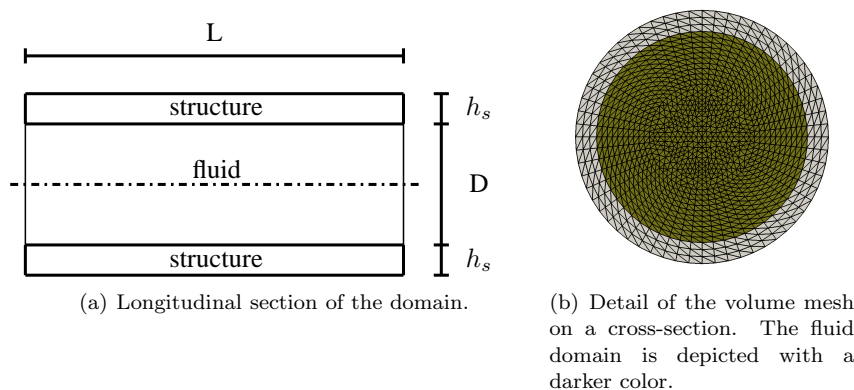


FIGURE 10. Computational domain for the FSI benchmark.

The motion of the fluid filling the deformable tube is described by the incompressible Navier-Stokes equations in ALE formulation (22)-(23), with $\rho_f = 1000$ kg/m³ and $\mu_f = 0.004$ Pa·s. The motion of the elastic shell is described by the elastodynamics equations (12), with $\mu_s = 5.77 \cdot 10^5$ Pa and $\lambda_s = 3.85 \cdot 10^5$ Pa (correspondingly, $E = 10^5$ Pa and $\nu_s = 0.3$). The coupled fluid-structure system is initially at rest and the wave propagation is initiated by setting $p = 500$ Pa at the fluid domain inlet for all $t > 0$. At the fluid domain outlet and on the outer structure wall, a stress-free boundary condition is imposed. Axial movements of the structure are prevented by prescribing a zero velocity in the axial direction on the inlet section.

The pressure step applied at the inlet causes a pressure wave to propagate down the tube. This induces a radial motion of the elastic structure, that shows a time history of damped oscillations around an asymptotic steady state. The frequency f of the oscillations and the steady state value of the radial displacement \bar{d}_r can be quantified as

$$f = \frac{1}{2\pi} \sqrt{\frac{4E}{D^2 \rho_s (1 + M_{fs})}}, \quad \bar{d}_r = \frac{D^2 p}{4E h_s}.$$

In the definition of f we use the ratio of equivalent fluid mass to solid mass M_{fs} , that depends on the mass of fluid contributing to the radial motion. For the problem at hand, we assume that only a fraction of the fluid mass contributes to the radial motion, and we set $M_{fs} = D/(8h_s)\rho_f/\rho_s$ [20]. This value for the equivalent mass

assumes a linear distribution of the radial fluid velocity. Finally, we obtain $M_{fs} = 1.67$, $f = 106.1$ Hz and $\bar{d}_r = 0.25$ mm.

An analytical solution for wave speed c can be given as a function of the geometric features, fluid and structure physical parameters of the system:

$$(34) \quad c = \phi \sqrt{\frac{K_f}{\rho_f} \left[1 + \left(\frac{(D + 2h_s)^2}{h_s(D + h_s)} - 2(1 - \nu_s) \right) \frac{K_f}{E} \right]^{-1}},$$

with

$$\phi = \sqrt{1 - \nu_s^2 \left[1 + \frac{E}{K_f} \frac{h_s}{D} \left(1 - \frac{K_f \rho_s}{E \rho_f} \right) \right]^{-1}}.$$

To the purpose of finding an analytical solution, the fluid was considered slightly compressible, with bulk modulus $K_f = 2.2 \cdot 10^9$ Pa. For the test case, $\phi = 0.95$ and $c = 2.77$ m/s.

The velocity of the fluid along the tube axis is predicted by Joukowski's equation [54]

$$u_x = \frac{p}{\rho_f c}$$

where p is the pressure gradient. In the case at hand $u_x = 18.02$ cm/s.

We present the comparison between the computed and analytical solutions of the proposed benchmark problem, evaluating the mismatch with respect to each quantity of interest. Following [20], we perform a series of numerical experiments, incrementally reducing the mesh size in the radial and axial directions. We identify the different meshes with a triplet of numbers, corresponding to the number of subdivisions in the axial direction, in the radial direction within the fluid domain, and in the thickness of the tube wall. We construct four meshes with the software GMSH, guaranteeing axial symmetry of the position of the mesh nodes. Each mesh contains an unstructured region, bounded by a cylinder of radius 1cm; outside that cylinder the mesh is structured, and the number of subdivisions in the circumferential direction is such that mesh elements at the interface between the structured and unstructured regions have a small shape factor (see Fig. 10(b)). Here follows the list of considered meshes:

- mesh 20-10-2, yielding a total number of degrees of freedom of about $1.5 \cdot 10^3$.
- mesh 30-20-3, yielding a total number of degrees of freedom of about $3.2 \cdot 10^3$.
- mesh 50-30-5, yielding a total number of degrees of freedom of $1.2 \cdot 10^6$.
- mesh 70-40-7, yielding a total number of degrees of freedom of about $2.9 \cdot 10^6$.

To compare the computed features of the propagating wave with the theoretical predictions, we limit our analysis to a time interval in which we can neglect the effects of reflected pressure waves from the outlet section. This limitation can be in principle removed, for instance by devising non-reflective boundary conditions (see e. g. [55]). However, we did not investigate this. As shown in Fig. 11, the wave has reached the outlet section at $t = 20$ ms. We therefore consider the results of our numerical experiments only in the time range $t \in (0, 20)$ ms.

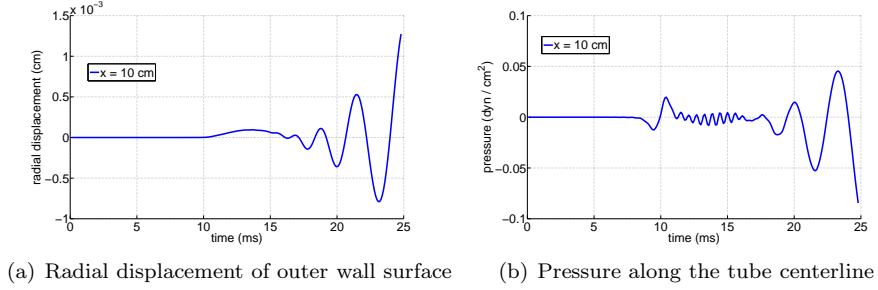


FIGURE 11. Time history at the outlet section (abscissa = 10 cm) of the (a) radial displacement of the outer wall and (b) fluid pressure on the tube axis. Around $t = 0.02$ s the propagating wave reaches the outlet section and wave reflections take place. Results obtained on the finest mesh were processed to generate these images.

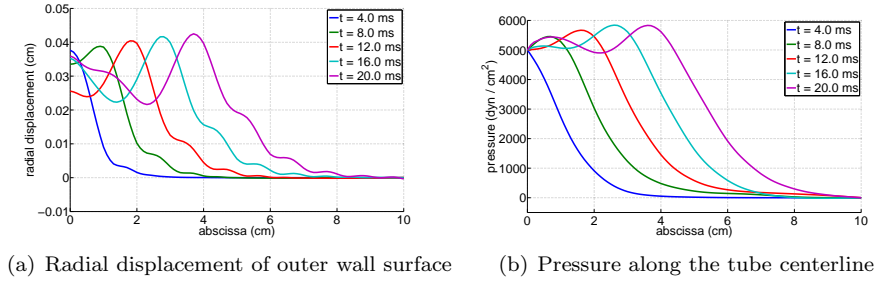


FIGURE 12. The wave propagation in the fluid and solid domains. Snapshots at different times of (a) the radial displacement of the outer wall surface (b) the fluid pressure along the tube centerline. Results obtained on the finest mesh were processed to generate these images.

TABLE 4. Predicted pressure wave speed from numerical experiments with different mesh size.

mesh	20-10-2	30-20-3	50-30-5	70-40-7
pressure wave speed (cm/s)	274.1983	275.3064	276.4382	276.6159

Fig. 12 shows the time history of the radial displacement of the structure computed with the finest mesh. The oscillations tend to damp to a constant steady state close to the value predicted by the analytical solution ($\simeq 0.25$ mm).

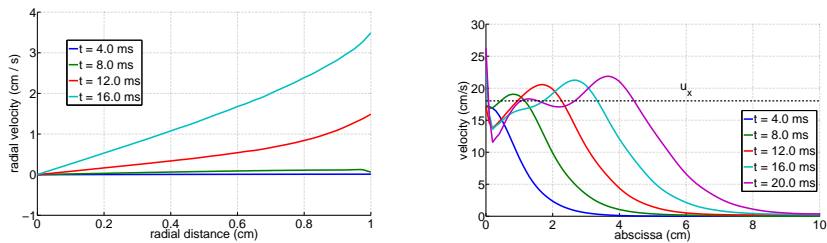
To compute the average pressure wave speed we first define the wave front at the half-height of the pressure step, or 250 Pa (see [20]); then we fit a first order polynomial to the position of the wave front in the time range $t \in (0, 20)$ ms and compute its (constant) derivative. The resulting estimate is not sensitive to the mesh size, and approximates the exact value of 2.77 m/s within a 1% error margin.

Table 4 shows the predicted wave speed from different numerical simulations with different grid sizes.

As a measure of the half-period of the wave we consider the distance between the first peak and the first valley in the pressure time plot. From the results obtained on the finest mesh we obtain for this value an estimate of 26 mm. Knowing the wave speed, we compute the wave frequency as 106.5 Hz, within 1% error from the analytical prediction.

We noted before that the theoretical value for the wave frequency depends on M_{fs} . The validity of our choice of M_{fs} can be checked on the computed results. Consistently with our assumption, Fig. 13 (a) shows in fact that the radial velocity of the fluid is a linear function of the radial position on a cross section at abscissa 5 cm, apart from a thin layer close to the wall (radius larger than 0.8 cm).

Finally, the axial velocity of the fluid, evaluated on the tube axis, is also a good approximation of the value predicted by Joukowski’s equation, as shown in Fig. 13 (b).



(a) Radial velocity on a cross-section at $x = 5$ cm (b) Axial velocity, compared with the Joukowski velocity u_x

FIGURE 13. The simulated wave propagation phenomenon matches closely theoretical predictions. Consistently with our assumptions on the model, the radial velocity of the fluid is a linear function of the radial position apart from a thin layer near the tube wall. The fluid velocity on the axis of the pipe approximates the value predicted by Joukowski’s equation. Results obtained on the finest mesh were processed to generate these images.

4. CONCLUSIONS

The main goal of this work is to describe an open source framework for the solution of flow problems relevant to biomechanics. At the core of this framework we place the software tools that we use to build the computational mesh (*pre-processing* phase); LifeV, the library of algorithms and data structures that we use to solve the differential problems (*processing* phase); software for the *post-processing* of the results of the numerical experiments.

Crucial aspects for a CFD framework are its *verification* and *validation*. We show in this paper how our tools can be tested against published benchmark problems for flow in rigid and deformable domains. Within this context, we also believe that it is important to provide a detailed account on the methods that we used, discussing where possible their merits and shortcomings.

In the simulation of flow in transitional and turbulent regimes, we addressed the issue of accuracy in the numerical integration performed by our code, pointing out the potential dramatic effect on the quality of the solution. The importance of the mesh has also been discussed, in particular its consistency with the symmetry of the physical problem. The flexibility of the mesh generator is therefore a key factor. Computational costs have been shown to be significant, as expected, in particular for flow regimes characterized by high values of the Reynolds number. While this is not an intrinsic limitation of the proposed framework, it is certainly an area of possible improvement, for instance through the implementation of effective turbulence models.

An important outcome of this work is the production of a suite of scripts and codes that are based on a completely open-source set of tools, and therefore can be readily shared with the community. As a matter of fact, we will prepare a distribution of our software that will be published through the web portal www.lifev.org and will allow the reproduction of the results presented in this paper.

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